

Monte Carlo calculated correction factors for a proton calorimeter in clinical proton beams

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Background



- Quantity of interest in clinical proton beams is **absorbed dose to water** but...
- ... to date, no primary standards laboratory has a proton or ion beam in which to conduct calibrations
- Current standard methods typically involve the use of an ionization chamber calibrated in a ⁶⁰Co beam – so a beam quality correction factor is needed to account for the difference between the chamber response in the proton/ion and the calibration beams.



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- This approach gives rise to uncertainties (at 68% confidence level) on the reference dosimetry of 2.3% for proton beams and 3.4% for carbon ion beams when using a plane-parallel ionization chamber (ref TRS-398).
- It has long been recognised and indeed stated in TRS 398 that the preferred method of calibration is to <u>calibrate chambers in a similar beam to that which is</u> <u>being used therapeutically</u>.
- A **new UK code of practice** is being written to facilitate calibration in proton beams primarily for scanned but also for scattered beam delivery modes.
- The aim is to deliver an uncertainty on reference dosimetry for protons of approximately 2% (at 95% CL) and will utilise a primary standard graphite calorimeter that is robust and portable enough to be used in the end-user facility.

Formalism based on the new CoP

- Water and graphite calorimeters have been developed & demonstrated in p beams
- Graphite calorimetry:
 - lots of <u>benefits</u> however largest uncertainty in absorbed dose-to-water determination is conversion of dose-to-graphite to dose-to-water

$$N_{D,w} = \frac{D_g}{M_g} \frac{s_{w,air}}{s_{g,air}} \frac{p_w}{p_g} \qquad z_{ref,g} = z_{ref,w} \frac{r_{g,80}}{r_{w,80}}$$
$$D_g = \left(\frac{E_{core}^{rad}}{m_{core}}\right) \cdot k_{imp} \cdot k_{non-g} \cdot k_{gap} \cdot k_{vol}$$
$$\left[k_{gap} \rightarrow gap \ correction \ factor \\ k_{vol} \rightarrow volume \ averaging \ correction$$

- Aim: determine k_{gap} and k_{vol} with Monte Carlo simulations using TOPAS (framework based on Geant4) for:
 - monoenergetic pencil beams
 - reference clinical SOBP beams (scanning/passive)





How do we calculate k_{qap} and k_{vol} ? Representative drawings

Not to scale !



Full geometry

Compensated geometry

$k_{vol} = D_{disk \ comp} / D_{core_comp}$



Compensated geometry Compensated + disc

TOPAS application (based on Geant4 v10.3.p01)

- Default modular physics list:
 - Hadronic: QGSP_BIC_HP (Binary Intra.Cascade)
 - *EM:* emstandard_opt4
 - ICRU90 material definitions
 - Production cuts 0.05mm
- Scoring/tracking: TOPAS
 - Total dose deposited per event
 - Standard deviation \rightarrow SDOM



Correction factors for mono energetic protons



250



- 3 cm beam diam & NO BU: k_{gap} upto 1.004 (230 MeV)
- 3 cm beam diam & 2.0 g/cm² BU: k_{gap} upto 1.008 (230 MeV)
- consistency with previous work (Petrie et al. 2016)
- no significant dependence of k_{gap} on I (78 vs 81 eV)
- Large beam diam (LSCPE), k_{gap} within 0.1% of unity for all the energies
- Large beam diam (LSCPE) and changing BU, <u>no</u> significant change

- Various disk thickness investigated
- k_{vol} ~ 0.997 at 60 MeV up to ~ 1.003 at 230 MeV
- Large beam diam & changing BU, <u>no significant</u> <u>change</u>

Clinical relevant SOBPs



 N^{32}

24 26 28

According to the new UK Code of Practice (*still in draft*), reference dosimetry has to be carried out in a STV (Standard Test Volume) centred at 15 cm depth in water (box 10 x 10 x 10 cm³)



8 10 1

0

18 20

nm)

2

Positive suitable solutions

Correction factors for SOBP



- Weighted using pencil beams on large slabs
- 10x10 cm² beam required by CoP
- Reciprocity theorem to be demonstrated
- 32 peaks in total \rightarrow uniformity within 0.5%
- Weights converted to numbers of events per peak in TOPAS

k _{gap}	k _{vol}
1.0006 ± 0.0005	1.0003 ± 0.0011



Correction factors for a passive beamline (CCC) **NP**

- NATIONAL Physical Laboratory
- Passive beam line for eye melanoma treatment with 62 MeV proton beams at the Clatterbridge Cancer Centre



- Weighted using pencil beams on large slabs
- 33 peaks in total \rightarrow uniformity within 0.5%

k _{gap}	k _{vol}
1.0024 ± 0.0015	?? ± ??





(still in progress!!!)

Summary and future work



Summary

- Overview of the formalism for determining absorbed dose to water in proton beams based on a new UK code of practice using a portable primary standard graphite calorimeter
- Description of methods for determining the *k_{gap}* and *k_{vol}* corrections with TOPAS (Geant4) for mono-energetic and clinical relevant beams
- For mono-energetic beams (LSCPE):

 k_{gap} within 0.1% of unity, $k_{vol} \sim 0.997$ at 60 MeV to ~ 1.003 at 230 MeV with <u>no significant change</u> with energy and build-up

• For the STV volume:

 $k_{gap} = 1.0006 \pm 0.0005$ $k_{vol} = 1.0003 \pm 0.0011$

• CCC

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k_{oap} = 1.0024 \pm 0.0015 k_{vol} = ?? \pm ?? (in progress!)
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Future work

- Improve the procedure for SOBP potentially decreasing the ripple and including more peaks
- Secondary STVs according to the new code of practice
- We want to establish a primary standard for reference proton dosimetry in preparation for the new proton centres in the UK in 2018



Thank you

Calorimetry our primary standard for radiation dosimetry are calorimeters



